Dynamic Causal Modelling for EEG/MEG: principles

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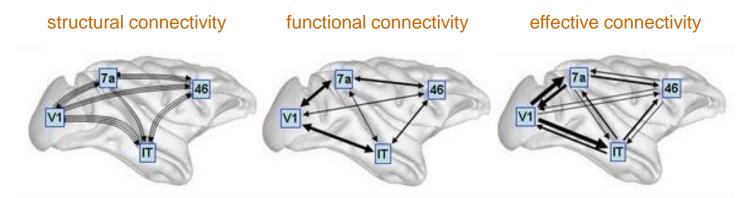
Overview

- 1 DCM: introduction
- 2 Dynamical systems theory
- 3 Neural states dynamics
- 4 Bayesian inference
- 5 Conclusion

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structural, functional and effective connectivity



O. Sporns 2007, Scholarpedia

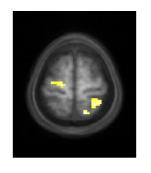
- structural connectivity
 - = presence of axonal connections
- functional connectivity
 - = statistical dependencies between regional time series
- effective connectivity
 - = causal (directed) influences between neuronal populations

! connections are recruited in a context-dependent fashion

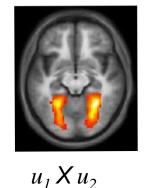
from functional segregation to functional integration

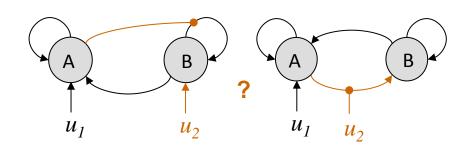
localizing brain activity: functional segregation

effective connectivity analysis: functional integration



 u_1

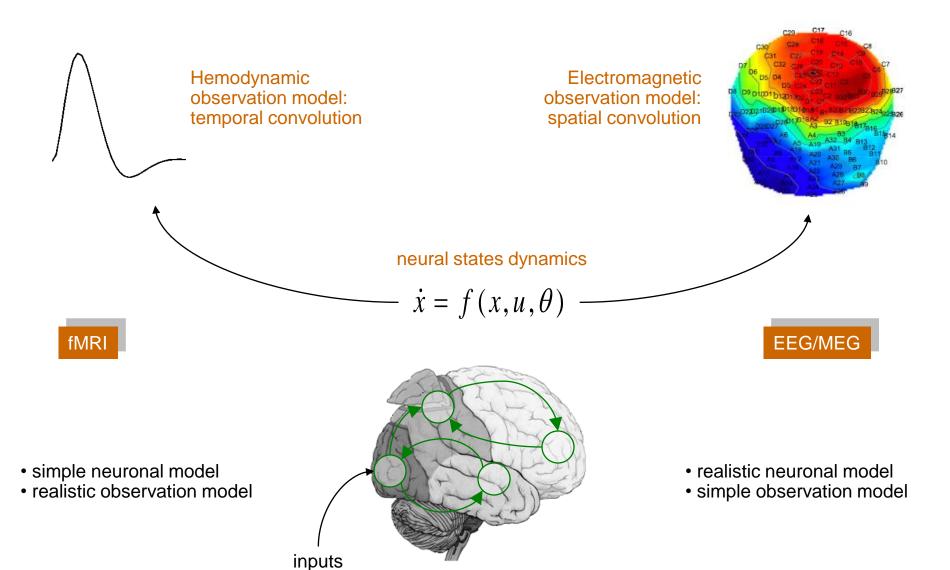




« Where, in the brain, did my experimental manipulation have an effect? »

« How did my experimental manipulation propagate through the network? »

DCM: evolution and observation mappings

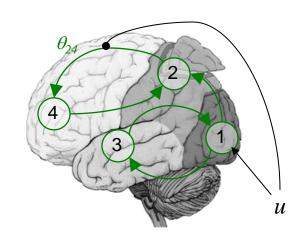


DCM: a parametric statistical approach

DCM: model structure

$$\begin{cases} y = g(x, \varphi) + \varepsilon \\ \dot{x} = f(x, u, \theta) \end{cases}$$

likelihood
$$\Rightarrow p(y|\theta,\varphi,m)$$



• DCM: Bayesian inference

parameter estimate:

$$\hat{\theta} = E[\theta | y, m]$$

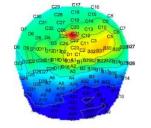
$$p(y|m) = \int p(y|\theta, \varphi, m) p(\theta|m) p(\varphi|m) d\varphi d\theta$$

DCM for EEG-MEG: auditory mismatch negativity

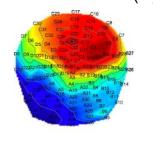
sequence of auditory stimuli



standard condition (S)

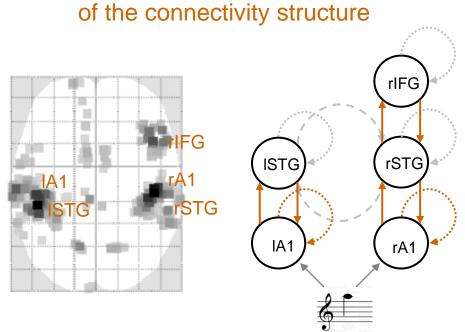


deviant condition (D)

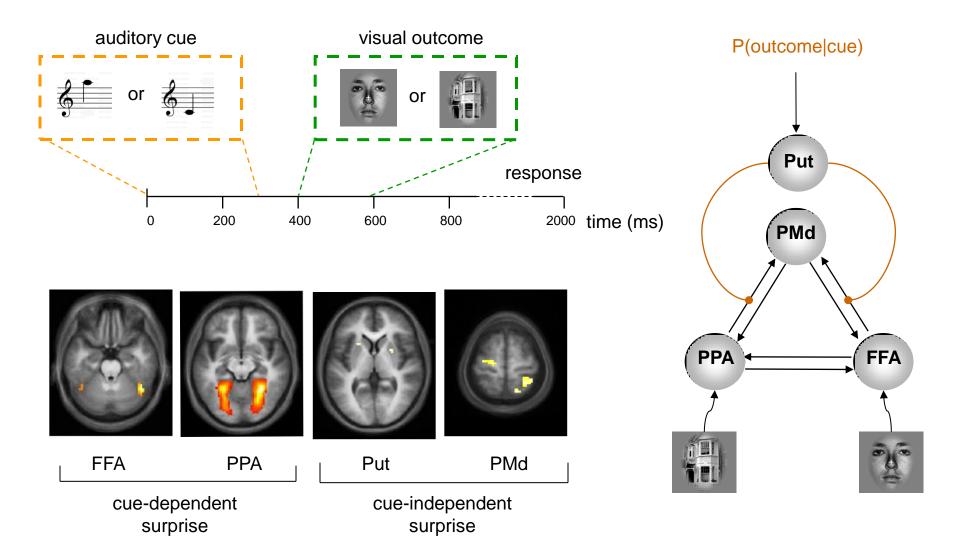


t ~ 200 ms

S-D: reorganisation



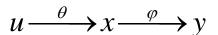
DCM for fMRI: audio-visual associative learning

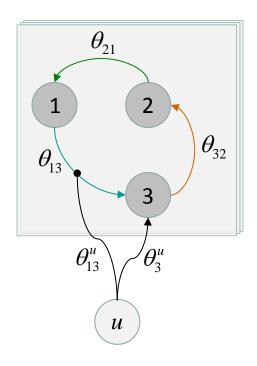


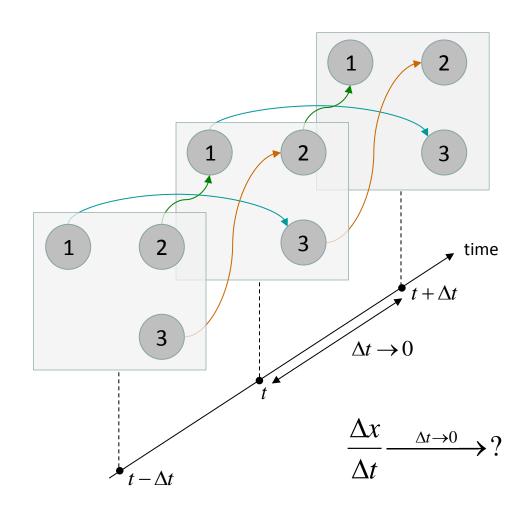
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motivation







Dynamical systems theory exponentials

We use the following shorthand for a time derivative

$$\dot{X} = \frac{dX}{dt}$$

The exponential function $x = \exp(t)$ is invariant to differentiation. Hence

$$\dot{x} = \exp(t)$$

and

$$\dot{X} = X$$

Hence exp(t) is the solution of the above differential equation.

initial values and fixed points

An exponential increase (a > 0) or decrease (a < 0) from initial condition x_0

$$x = x_0 \exp(at)$$

has derivative

$$\dot{x} = ax_0 \exp(at)$$

The top equation is therefore the solution of the differential equation

$$\dot{x} = ax$$

with initial condition x_0 .

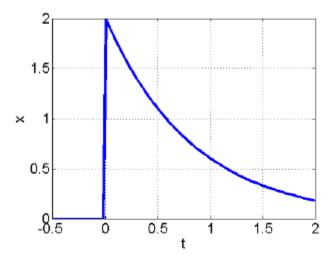
The values of x for which $\dot{x} = 0$ are referred to as Fixed Points (FPs). For the above the only fixed point is at x = 0.

time constants

The figure shows

$$\dot{x} = ax$$

with a = -1.2 and intial value $x_0 = 2$.



The time constant is $\tau = -1/a$.

The time at which x decays to half its initial value is

$$\tau_h = \frac{1}{a} \log(1/2)$$

which equals $\tau_h = 0.58$.

matrix exponential

If x is a vector whose evolution is governed by a system of linear differential equations we can write

$$\dot{x} = Ax$$

where A describes the linear dependencies.

The only fixed point is at x = 0.

For initial conditions x_0 the above system has solution

$$x_t = \exp(At)x_0$$

where $\exp(At)$ is the matrix exponential (written expm in matlab) (Moler and Van Loan, 2003).

eigendecomposition of the Jacobian

The equation

$$\dot{x} = Ax$$

can be understood by representing A with an eigendecomposition, with eigenvalues λ_k and eigenvectors q_k that satisfy (Strang, p. 255)

$$A = Q \Lambda Q^{-1}$$

We can then use the identity

$$\exp(A) = Q \exp(\Lambda) Q^{-1}$$

Because Λ is diagonal, the matrix exponential simplifies to a simple exponential function over each diagonal element.

dynamical modes

This tells us that the original dynamics

$$\dot{x} = Ax$$

has a solution

$$x_t = \exp(At)$$

that can be represented as a linear sum of k independent dynamical modes

$$x_t = \sum_k q_k \exp(\lambda_k t)$$

where q_k and λ_k are the kth eigenvector and eigenvalue of A. For $\lambda_k > 0$ we have an unstable mode.

For λ_k < 0 we have a stable mode, and the magnitude of λ_k determines the time constant of decay to the fixed point.

The eigenvalues can also be complex. This gives rise to oscillations.

Dynamical systems theory spirals

A spiral occurs in a two-dimensional system when both eigenvalues are a complex conjugate pair. For example (Wilson, 1999)

$$\begin{bmatrix} \dot{X}_1 \\ \dot{X}_2 \end{bmatrix} = \begin{bmatrix} -2 & -16 \\ 4 & -2 \end{bmatrix} \begin{bmatrix} X_1 \\ X_2 \end{bmatrix}$$

has

$$\lambda_1 = -2 + 8i$$
$$\lambda_2 = -2 - 8i$$

giving solutions (for initial conditions $x = [1, 1]^T$)

$$x_1(t) = \exp(-2t) [\cos(8t) - 2\sin(8t)]$$

 $x_2(t) = \exp(-2t) [\cos(8t) + 0.5\sin(8t)]$

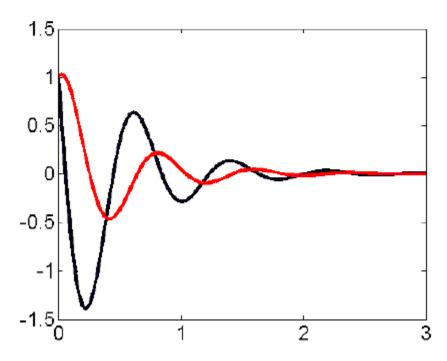
Dynamical systems theory spirals

We plot time series solutions

$$x_1(t) = \exp(-2t)(\cos(8t) - 2\sin(8t))$$

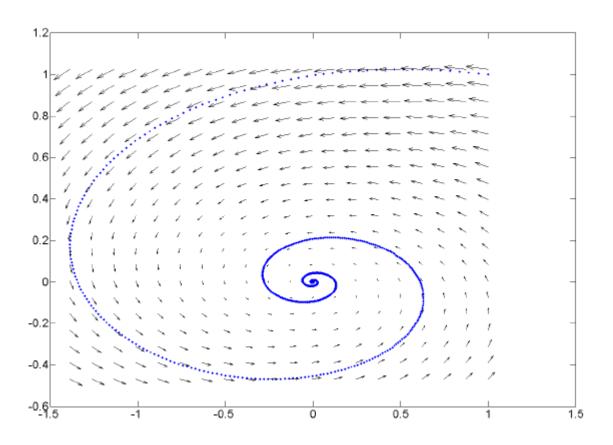
 $x_2(t) = \exp(-2t)(\cos(8t) + 0.5\sin(8t))$

for x_1 (black) and x_2 (red).



spiral state-space

Plotting x_2 against x_1 gives the state-space representation.



Dynamical systems theory embedding

Univariate higher order differential equations can be represented as multivariate first order DEs.

For example

$$\ddot{V} = \frac{H}{\tau} u_t - \frac{2}{\tau} \dot{V} - \frac{1}{\tau^2} V$$

can be written as

$$\dot{c} = c
\dot{c} = \frac{H}{\tau} u_t - \frac{2}{\tau} c - \frac{1}{\tau^2} V$$

kernels and convolution

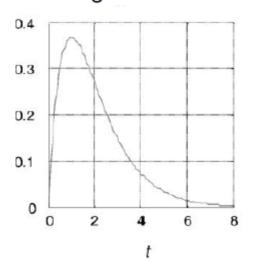
The previous differential equation has a solution given by the integral

$$v(t) = \int u(t)h(t - t')dt'$$

where

$$h(t) = \frac{H}{\tau} t \exp(-t/\tau)$$

is a kernel. In this case it is an alpha function synapse with magnitude H and time constant τ

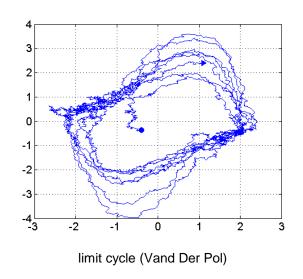


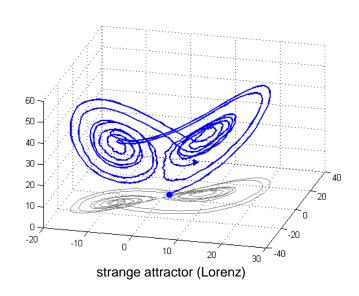
The previous integral can be written as

$$v = u \otimes h$$

Dynamical systems theory summary

- Motivation: modelling reciprocal influences
- Link between the integral (convolution) and differential (ODE) forms
- System stability and dynamical modes can be derived from the system's Jacobian:
 - D>0: fixed points
 - D>1: spirals
 - D>1: limit cycles (e.g., action potentials)
 - D>2: metastability (e.g., winnerless competition)

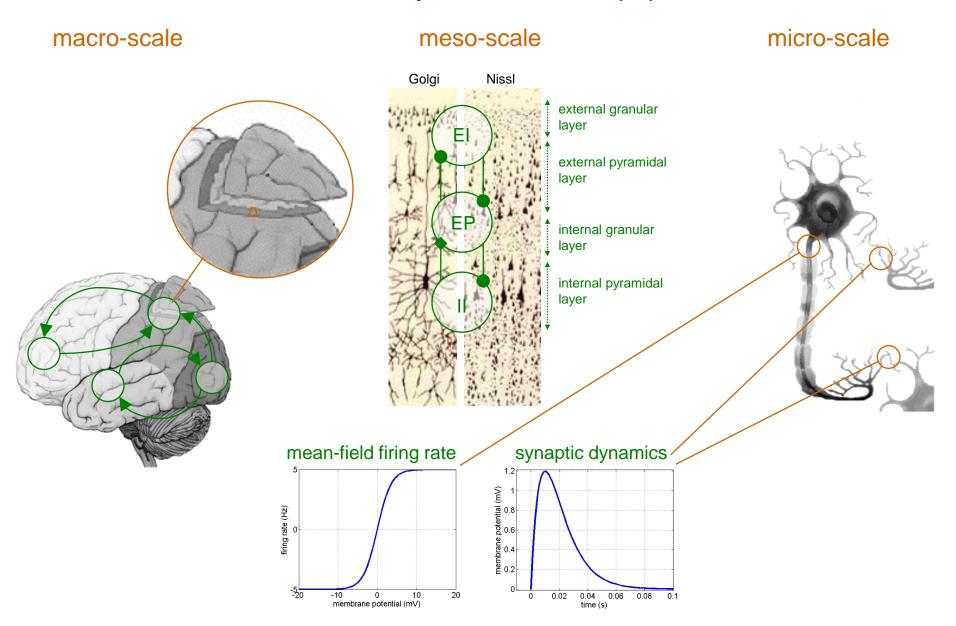




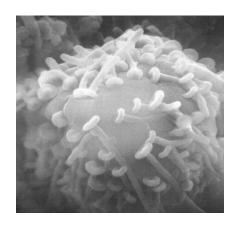
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DCM for M/EEG: systems of neural populations



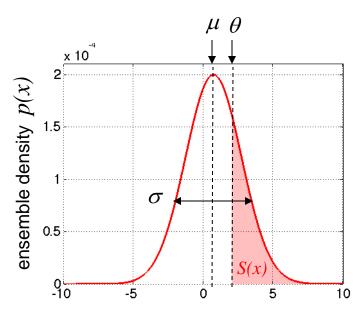
DCM for M/EEG: from micro- to meso-scale



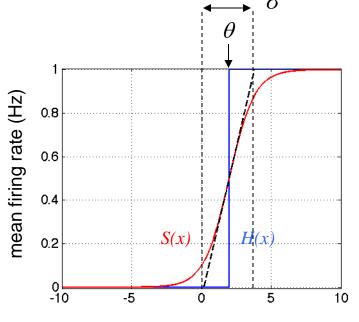
 $x_{i}(t)$: post-synaptic potential of j^{th} neuron within its ensemble

$$\frac{1}{N-1} \sum_{j' \neq j} H\left(x_{j'}(t) - \theta\right) \xrightarrow{N \to \infty} \int H\left(x(t) - \theta\right) p\left(x(t)\right) dx$$

$$\approx S\left(\mu\right) \text{ mean-field firing rate}$$

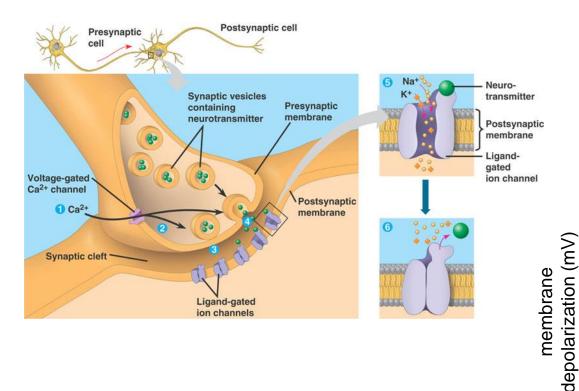


membrane depolarization (mV)



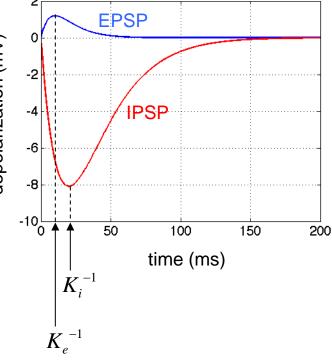
mean membrane depolarization (mV)

DCM for M/EEG: synaptic dynamics

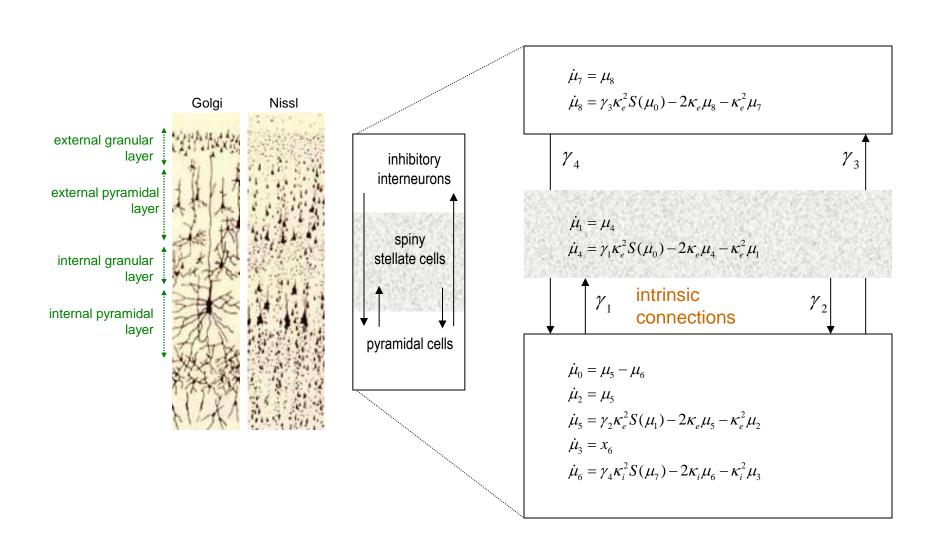


$$\begin{cases} \dot{\mu}_1 = \mu_2 \\ \dot{\mu}_2 = \kappa_{i/e}^2 S(\bullet) - 2\kappa_{i/e} \mu_2 - \kappa_{i/e}^2 \mu_1 \end{cases}$$

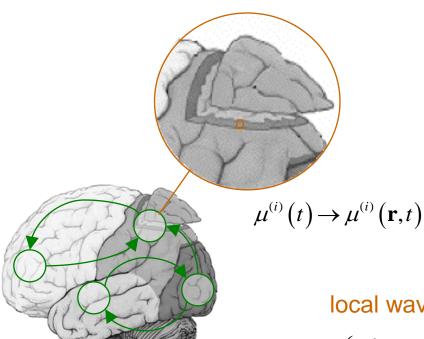
post-synaptic potential

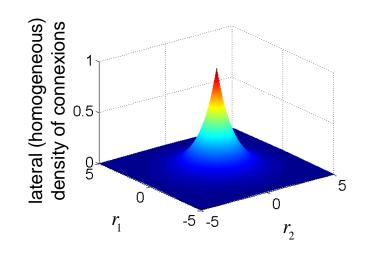


DCM for M/EEG: intrinsic connections within the cortical column



DCM for M/EEG: from meso- to macro-scale

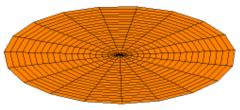




local wave propagation equation (neural field):

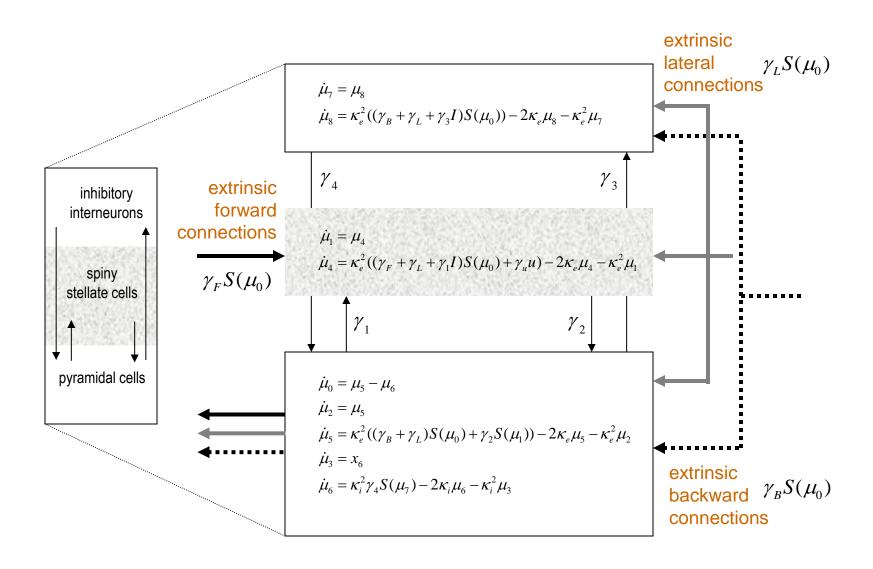
$$\left(\frac{\partial^{2}}{\partial t^{2}} + 2\kappa \frac{\partial}{\partial t} + \kappa^{2} - \frac{3}{2}c^{2}\nabla^{2}\right)\mu^{(i)}(\mathbf{r}, t) \approx c\kappa \varsigma^{(i)}(\mathbf{r}, t)$$

$$\varsigma^{(i)} = \sum_{i'} \gamma_{ii'} S(\mu^{(i')})$$



0th-order approximation: standing wave

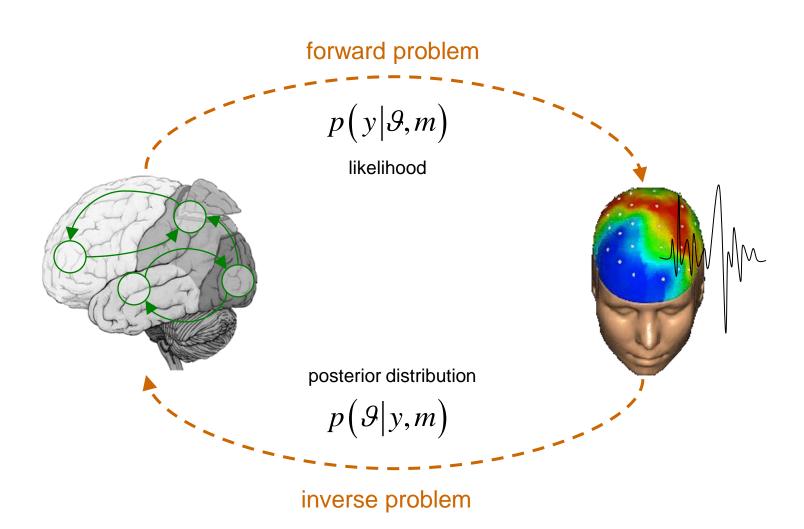
DCM for M/EEG: extrinsic connections between brain regions



Overview

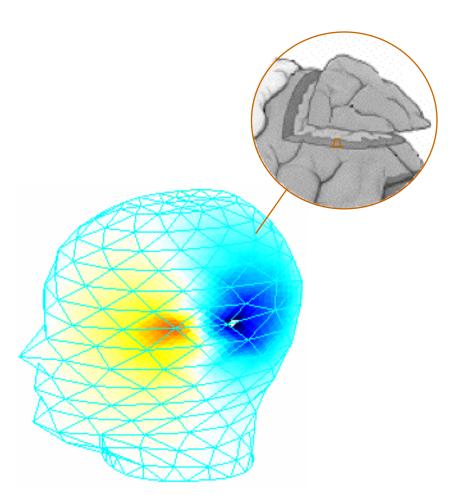
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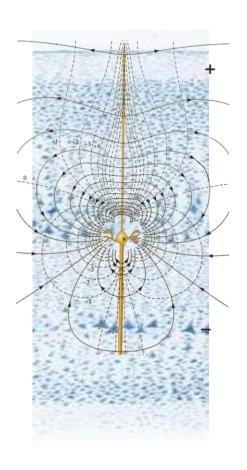
forward and inverse problems



the electromagnetic forward problem

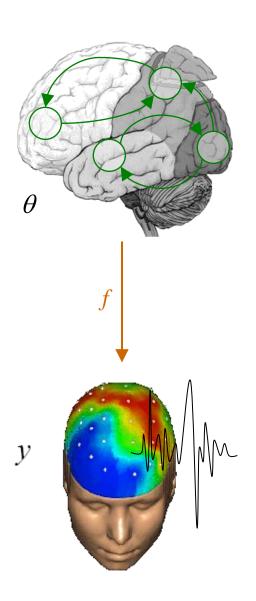
$$\mathbf{y}(t) = \sum_{i} \mathbf{L}^{(i)} \mathbf{w}_{0}^{(i)} \sum_{j} \beta_{j} \mu^{(ij)}(t) + \varepsilon(t)$$





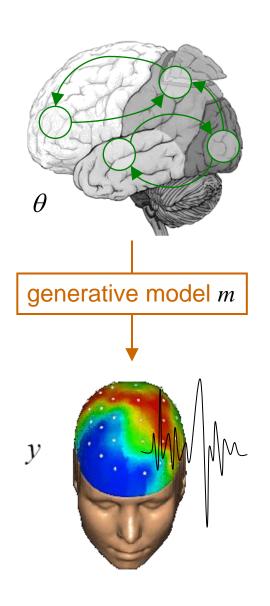
Bayesian paradigm

deriving the likelihood function



Bayesian paradigm

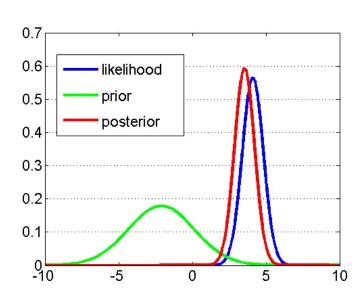
likelihood, priors and the model evidence



Likelihood: $p(y|\theta,m)$

Prior: $p(\theta|m)$

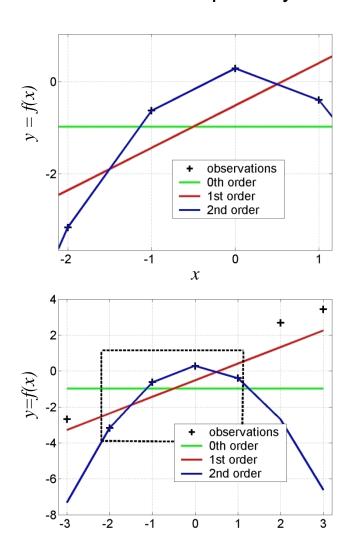
Bayes rule: $p(\theta|y,m) = \frac{p(y|\theta,m) p(\theta|m)}{p(y|m)}$



model comparison

Principle of parsimony:

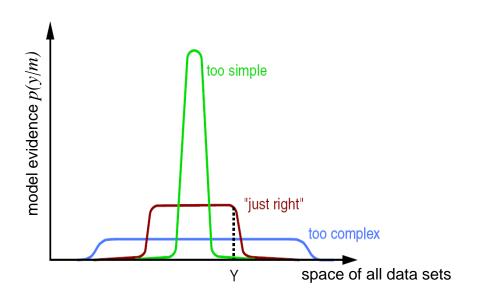
« plurality should not be assumed without necessity »



Model evidence:

$$p(y|m) = \int p(y|\theta,m) p(\theta|m) d\theta$$

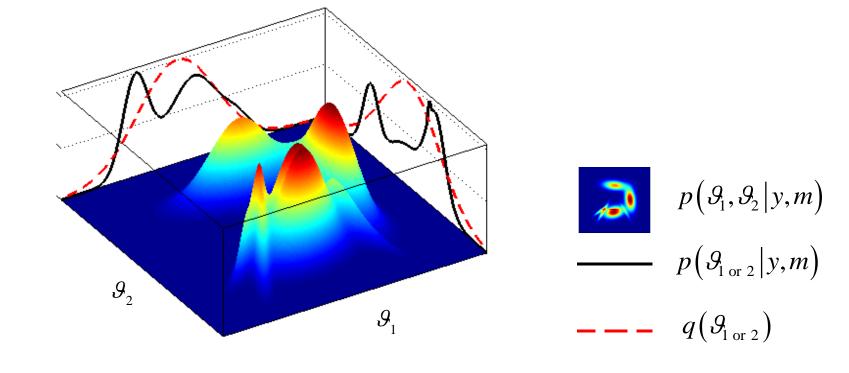
"Occam's razor":



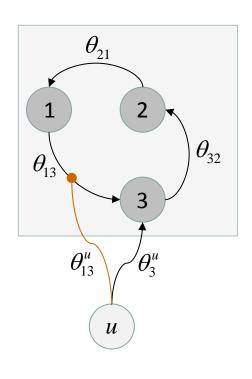
the variational Bayesian approach

$$\ln p(y|m) = \left\langle \ln p(\vartheta, y|m) \right\rangle_{q} + S(q) + D_{KL}(q(\vartheta); p(\vartheta|y, m))$$
free energy: functional of q

mean-field: approximate marginal posterior distributions: $\{q(\mathcal{G}_1), q(\mathcal{G}_2)\}$



DCM: key model parameters

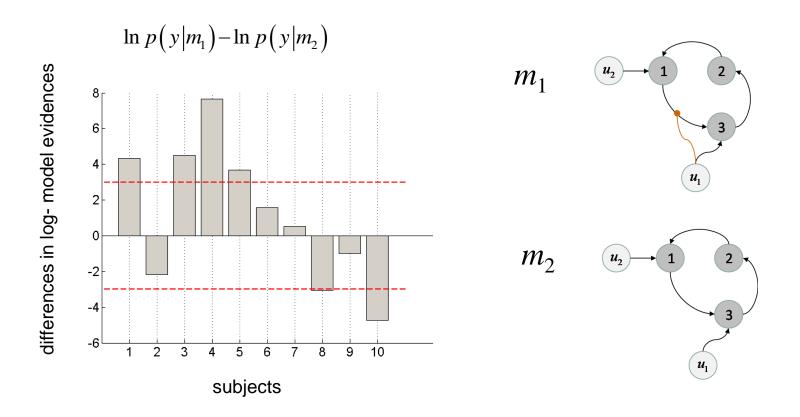


 $(\theta_{21}, \theta_{32}, \theta_{13})$ state-state coupling

 θ_3^u input-state coupling

 θ_{13}^u input-dependent modulatory effect

model comparison for group studies



fixed effect

assume all subjects correspond to the same model

random effect

assume different subjects might correspond to different models

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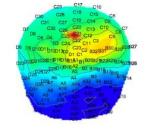
Conclusion

back to the auditory mismatch negativity

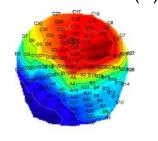
sequence of auditory stimuli



standard condition (S)



deviant condition (D)



t ~ 200 ms

S-D: reorganisation

of the connectivity structure

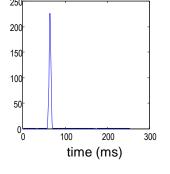
rIFG
ISTG
rSTG
IA1
rA1
ISTG
rA1
rA1

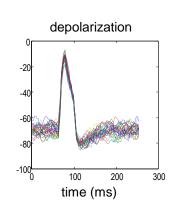
Conclusion

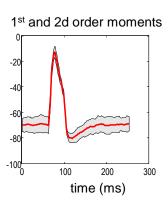
DCM for EEG/MEG: variants

input

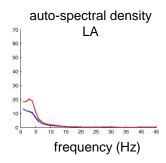
second-order mean-field DCM

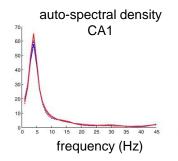


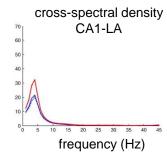




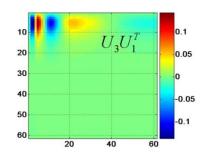
• DCM for steady-state responses

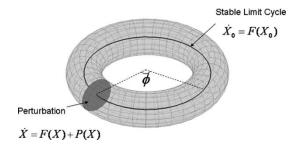






- DCM for induced responses
- DCM for phase coupling





Conclusion

planning a compatible DCM study

- Suitable experimental design:
 - any design that is suitable for a GLM
 - preferably multi-factorial (e.g. 2 x 2)
 - e.g. one factor that varies the driving (sensory) input
 - and one factor that varies the modulatory input
- Hypothesis and model:
 - define specific a priori hypothesis
 - which models are relevant to test this hypothesis?
 - check existence of effect on data features of interest
 - there exists formal methods for optimizing the experimental design for the ensuing bayesian model comparison
 [Daunizeau et al., PLoS Comp. Biol., 2011]

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